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3 1 AUG 2002

Request for grant of a patent

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3.	Full name, address and postcode of the or of each applicant (underline all surnames)	Professor Neil <u>Graham</u> 6 Kilmardinny Grove Bearsden	
	Patents ADP number (if you know it)	GLASGOW G61 3NY	
	If the applicant is a corporate body, give the country/state of its incorporation	·	
4.	Title of the invention	Novel thermoplastic h for use in producing of producing said com	ydrogel polymer composit contact lenses and metho positions
5.	Name of your agent (if you have one)	Kennedys Patent Agenc	cy Limited
	"Address for service" in the United Kingdom to which all correspondence should be sent (Including the postcode)	Floor 5, Queens House 29 St Vincent Place GLASGOW Gl 2DT	<b>2</b>
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7.	If this application is divided or otherwise derived from an earlier UK application, give the number and the filing date of the earlier application	Number of earlier application	Date of filing (day / month / year)
8.	Is a statement of inventorship and of right to grant of a patent required in support of this request? (Answer Yes if:  a) any applicant named in part 3 is not an inventor of there is an inventor who is not named as an applicant, or  c) any named applicant is a corporate body.	No .	·

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Description

11

Claim (s)

Abstract

CF

Drawing (s)

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**Priority documents** 

Translations of priority documents

Statement of inventorship and right to grant of a patent (Patents Form 7/77)

Request for preliminary examination and search (Patents Form 9/77)

Request for substantive examination (Patents Form 10/77)

Any other documents (please specify)

11.

I/We request the grant of a patent on the basis of this application.

Kennedys

Date

30 August 2002

12. Name and daytime telephone number of person to contact in the United Kingdom

Claire Rutherford

0141 226 6826

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```
Novel Thermoplastic Hydrogel Polymer Compositions for use
1
    in producing contact lenses and Methods of Producing said
2
3
    Compositions
4
    The present invention relates generally to production of
5,
    thermoplastic hydrogels for use as contact lenses.
6
    particular, the invention relates to thermoplastic
7
    hydrogels which show improved flow characteristics.
8
9
    It is already known in the art to make contact lenses
10
    using hydrogels. Generally these hydrogels are HEMA, NVP
11
    or products of free radical polymerisation. However,
12
    these compositions generally do not flow and can only be
13
    moulded by reaction injection moulding (RIM), which is a
14
    slow and relatively expensive process which is not
15
    particularly suited to contact lens manufacture.
16
17
    Also, existing reaction injection moulding techniques
18
    utilise free radical initiation or irradiation cure that
19
    produces radicals. These radicals initiate a
20
    peroxidation chain process, which leads ultimately to
21
    damage of PEO based polymers in storage for use which
22
    gives a short life to contact lenses produced from them.
23
```

2

1 There are also problems with bio-compatibility of 2 reaction injection moulded hydrogels which again is not ideal for the manufacture of contact lenses where bio-3 4 compatibility is importantant. 5, 6, Additionally, the current cross linked polymer hydrogels 7 often have a very poor resistance to crack initiation and 8 crack propagation which again can be problematic when C) producing contact lenses. 10 11 It can therefore be seen that it would be beneficial to 12 provide thermoplastic hydrogels which are capable of being generally moulded under pressure so that contact 13 14 lenses can be easily and cheaply produced. 15 16 It is an aim of the present invention to provide a 17 thermoplastic hydrogel composition which has the ability to flow under moderate shear at particular temperatures 18 19 below the polymer decomposition temperature. 20 21 It is a further object of the present invention to 22 provide a thermoplastic hydrogel composition which can be 23 injection or compression moulded. 24 25 It is a further object of the present invention to provide a solvent soluble composition. 26 27 28 Another object of the present invention is to provide a 29 thermoplastic hydrogel composition which is highly bio 30 compatible. 31.

32 A yet further object of the present invention is to

33 provide thermoplastic hydrogels which have a high level

```
of water swelling properties after moulding and swelling
1
2
    with water.
 3:
    According to a first aspect of the present invention,
 4
    there is provided a method of producing thermoplastic
 5
    hydrogels for use in producing contact lenses, comprising
 6
    the steps of reacting one or more from the list;
 7
         polyethylene oxide,
 8
 ξı
         polyol,
         polyamine,
10
    with a polyisocyanate and a polyfunctional amine or
11
12
    alcohol.
13
    Preferably the polyol is polyethylene glycol.
14
15
    Preferably, the method also comprises the step of end
16
    capping unreacted groups with a unit capable of producing
17
    hydrogen bonding, \pi bonding, ionic boding and/or phase
18
     separation or forming a glassy phase separated domain.
19
20
     Alternatively, according to a second aspect of the
21
     present invention, the method also comprises the step of
22.
     end capping unreacted groups with a unit from a list of:
23
24
          Mono-functional amine
25
          Mono-functional isocyanate
26
          Monofunctional anhydride
27
          Acid
28
          Mono-functional hydroxyl
29
     Preferably the reaction between one or more from the list
30
31
          polyethylene oxide
32
          polyol
33
          polyamine
```

and a polyisocyanate is prepared using a range of NCO:OH 2 or NCO:NH ratios. 3 Optionally a biodegradable unit may be incorporated. 4 5 The biodegradable unit may be polycaprolactone, poly 6 (lactic acid), poly(glycolic) acid or 7 8 poly(hydroxybutyric)acid, amine or hyroxyl ended poly(amino) acids (protein or peptide analogues). 9 10 The ratios are preferably selected such that, at complete 11 12 reaction, the product does not form a macrogel. 13 14 Preferably the first step reaction is prepared using a range of NCO:OH OH or NCO:NH2 ratios from 2:1 to 1:2. 15 16 Most preferably the first step reaction is prepared using 17 NCO:OH OH or NCO:NH<sub>2</sub> ratios of 2.0:1 to 1:1.8 and 1.8:1 to 18 19 1:1.8. 20 21 Optionally the range of ratios used may be extended by 22 the addition of monofunctional amines, alcohols or 23 cyanates. 24 25 Alternatively, a macrogel is prevented from forming by 26 stopping the reaction before completion. 27 28 Preferably, the reaction is stopped by the addition of a 29 monoamine or an amine terminated polymer.

3(1

31 Optionally, the monoamine or an amine terminated polymer

32 is added when the reaction is partially complete.

3.5

Alternatively, an amine is admixed at the outset thus 1 removing the possibility of gelation. 2 3 Preferably, the amine is added in the form of amine 4 5, carbonate. 6 Typically, products with NCO end groups are subjected to 7 a final curing by immersion in liquid water or steam 8 after moulding. 9 10 Preferably, in the second stage the unreacted groups are 11 capped with an amine. 12 13 Optionally, unreacted NCO groups are endcapped. 14 15 Another option is that unreacted OH groups are endcapped. 16 17 Preferably, terminal NCO groups are converted into a 18 strongly hydrogen bonding urea group. 19 20 Preferably, the unreacted groups are capped with an 21. aliphatic amine. 22 23 Optionally, the amine group is attached to a long linear 24 or branched alkyl group or to an aryl- or aralkyl-amine. 25 26 Optionally, the amine group is attached to polymers or 27 28 low molecular weight pre-polymers. 29 Alternatively, excess OH groups are capped with one or 30 more molecules from the list of; 31 mono-isocyanate ended aromatic molecules, 32.

mono-acid anhydride ended aromatic molecules,

6

- 1 mono-isocyanate ended aliphatic molecules,
- 2 mono-acid anhydride ended aliphatic molecules
- 3 reaction product of a monoamine with a di(or higher)
- 4 isocyanate.

5.

- 6 The groups used in the endcapping process allow the
- 7 polymers to interact with physical or chemical cross-
- 8 linking. The separate particles therefore bind to each
- 9 other.

10

- 11 According to the third aspect of this invention there is
- 12 provided a thermoplastic hydrogel for use in producing
- 13 contact lenses produced by the methods of the first and
- 14 second aspects.

15

- 16 Preferably, the hydrogel is completely polymerised under
- 17 the specific conditions that are being used.

18

19 Preferably, after polymerisation the hydrogel is heated.

20

- 21 Alternatively, after polymerisation the hydrogel is
- 22 immersed in water liquid or vapour.

23

- 24 Optionally, the end product may be pelletised, pressed,
- 25 extruded or heat, pressure, injection or compression
- 26 moulded.

27

- 28 Preferably, the end product incorporates an antioxidant
- 29 containing two or more hydroxyl groups.

3(1

31 The antioxidant may be internal or external.

32

33 Preferably, the antioxidant is ascorbic acid.

7 1 Alternatively, the antioxidant is 2,6-ditertiarybuty14-2 3 hyroxanisol. 4 Optionally, the end product can incorporate dye. 5 6 According to a fourth aspect of the present invention 7 there is provided a contact lens produced from the 8 hydrogel of the third aspect. 9 10 An example of the present invention will now be 11 illustrated by way of example only and with reference to 12 the following figure, in which: 13 14 Figure 1 shows typical end groups that could be envisaged 15 as being associated in stacks as shown. 16 17 In the preferred embodiment, the thermoplastic materials 18 are prepared from mixtures of di (or higher) PEG polyol 19 with a di (or higher) polyisocyanate and/or a di (or 20 higher) polyamine. 21 22 First stage materials can also be made from many step-23 growth reactions amongst which the reaction of PEG 24 polyols with polyacids with removal of reactive-produced 25 water is an option. The production of first stage 26 materials can also be guided by the art of making alkid 27 resins in the paint industry. 28 29 If the product from the first stage reaction is made from 30 a mixture of PEG diol, 1, 2, 6-hexantriol and 31 diphenylmethane-4,4-diisocyanate, it can be prepared 32 using a range of NCO:OH ratios from, for example, 2:1 to

1 At the extremes of these ratios, the 2:1 will have 2 all NCO unreacted groups and the 1:2 ratio will have all 3 OH unreacted groups. These compositions are not able to macrogel and will contain only small proportions of low 4 5 molecular rate branched polymers. The product is a fluid and suitable for injection, extrusion or compression 6 7 moulding at temperatures which are typically below 150°C, 8 although temperatures of 200°C to 250°C can be utilised 9 for short periods. It should be noted that the products with NCO end groups can only be moulded and subjected to 10 final curing by immersion in liquid water or steam for a 11 12 suitable period. 13 14 It is possible to use intermediate NCO:OH ratios, such as 2:1 to 1:1.8 and 1.8:1 to 1:1.8 (and these ranges can be 15 16 further extended by the addition of mono-functional 17 molecules). As these still provide at complete reaction, 18 fluid systems, which when the end groups, are NCO can be 19 injection moulded and post-cured by water or steam 20 However, depending on the proportion of tri 21 or higher functional materials, ratios such as 1.6:1 to 22 1:1.6 form macrogels at as complete a reaction as is 23 possible with the NCO and OH groups present (and less 24 extended ratios are possible if mono-functional amines, 25 alcohols or cyanates are used in the first stage. 26 resulting products are not fuseable and are not solvent 27 soluble). It is possible that the products may still be 28 used for the second stage of the process, to give useful 29 end capped products, if the reaction is stopped before it 30 has proceeded as far as possible. This operation is less 31 convenient and more difficult as the degree of completion 32 of the reaction must be determined using, for example,

infra-red analysis of the isocyanate absorption peak of

the reaction mixture; or by the viscosity of the reaction. Therefore, it is much preferred to use the 2 compositions which cannot macrogel, as they can be taken 3 to completion of the first stage without fear of irreversibly solidifying the reactants. Ŀ, 6 A preferred embodiment is that the first stage product is a heavily branched polyurethane/PEG resin. 8 embodiment, the second stage is intended to convert each C) of the terminal groups into a strongly hydrogen bonding 10 urea group. An aliphatic amine could be used and the 11. amine group could be attached to a short or long linear 12 or branched (preferably linear) alkyl group, such as 13 decyl or stearic or higher polyamines such as 14 polyethylene, or to an aryl or aralkylamine, such as 15 aniline, aminoanthracene or octylaniline. 16 combination of the urea group and the long aliphatic 17 chain or aromatic ring will promote association and phase 18 separation of these groups with development in the 19 product material of toughness and strength. 20 especially the case where an aromatic diisocyanate has 21. been utilised in stage one. 22. 23 Figure 1 shows a diagram of a typical end group which 24 could be envisaged as associating in stacks, as shown. 25 The association of many such end groups should provide 26 increased cohesion and strength to the product. 27 28 Once the initial homogeneous mixing has been completed, 29 then the still fluid mix may be poured into suitable 30 containers, such as polypropylene moulds. 31

polymerisation (curing) of the finished product can then be completed. In order to provide an oxidation resistant 33

product, it is particularly useful to incorporate a 1 2 reactive antioxidant containing two or more hydroxyl 3 groups, for example, ascorbic acid (alternatively an 4 external anti-oxidants may be used). Alternatively the 5 antioxidant may be added in earlier during the first 6 stage. 7 8 The final product can then be moulded into contact 9 lenses. The product has a number of benefits, in 10 particular as there will be no unreacted extractable . 11 groups left in the completed product, it is particularly 12 useful for contact lenses as it is bio-compatible. 13 is also the benefit that materials made from the final 14 hydrogel product which are soft and strong would be 15 comfortable and re-useable again something which is 16 particularly useful in contact lens manufacture. 17 final product would also have the benefit of being 18 intrinsically rubbery in their dry state, and therefore 19 contact lenses would not set rigid when dried out. Also, 20 coloured dyes can be put into the final product easily, 21 which cannot be done with similar cross-linked hydrogels 22 and this could be useful when making "fashion" contact 23 lenses, or sun protective or prosthetic contact lenses 24 which have colours, designs or dyes with particular 25 characteristics incorporated into them. 26 27 It can be seen that the embodiments disclosed are both or 28 merely exemplary of the present invention, which may be 29 embodied in many different forms. Therefore, details 30 disclosed herein are not to be interpreted as limiting, 31 but merely as a basis for the claims and for teaching one 32 skilled in art as to the various uses of the present 33 invention in any appropriate matter. In particular, it

should be noted that a wide variety of changes can be 1 made in this process. 2 3 For example, pre-polymers with excess OH can be capped 4 with a mono-isocyanate ended aromatic or aliphatic 5 molecule or with a reaction product of a mono-amine with 6 di or higher isocyanate. The low molecular weight amine 7 could be replaced with a low molecular weight polymeric 8 amine, such as low  $M_n$  primary and secondary amine ended Çì nylon polyamide) or polypropylene oxide, poly(butanediol) 10 or low molecular weight polymers producing glassy domains 11. such as end-capped polystyrenes or amine end-capped 12 hydrophobic and crystalline domain forms such as 13 poly(ethylene) units. The reaction can be between such 14 amine ended PEGs and PPGs and di or higher amines and di 15 or higher isocyanates, but done in solvents to allow 16 suitable reduced viscosity to be obtained. Also, to slow 17 down the amine reaction, the amine can be added at the 18 outset as the carbonate version of amine carbonate, 19 resulting from the reaction of amine and carbon dioxide. 20 21 Also, stage one hydroxlic excess polymers could be 22: reacted with a phase separating polymer end capped with 23 an anhydride group. 24 25 Finally, it should be noted that this end capping process 26 could be applied to a wide variety of polymers, such as 27 polyesters, nylons, polyurethanes, polyureas, polyethers,

polyolefins, polyvinyls and poly(meth)acrylates. 29

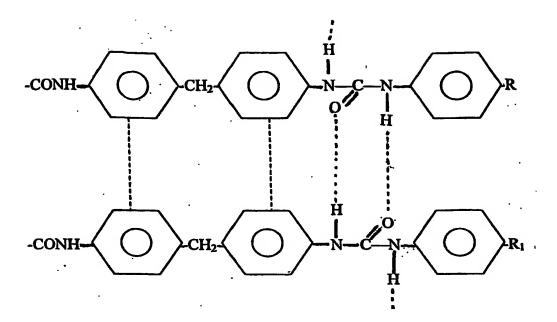


Fig 1

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